

# Effect of Repeated Firings on Color Stability of Repaired Zirconia

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## Research Article

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## ABSTRACT

**Aim:** The goal of this study was to investigate effect of repeated firings on color stability of repaired zirconia restorations.

**Materials and Methods:** Eighty disc shaped (dimensions: 2 mm x 5 mm) zirconia samples were fabricated using CAD/CAM technology. The samples were randomly divided into two groups for two different intraoral porcelain repair kits (Ceramic Repair N and Clearfil Repair). Four subgroups (n=10) were set at these groups according to number of firing (1, 3, 5 and 7). L\*a\*b\* values of the specimens were recorded and firing were performed in a porcelain furnace. After the firing process, specimens of each subgroup were repaired using a teflon mold (dimensions: 2 mm x 2 mm) with a porcelain repair kit that was related to major group and a compatible composite resin. L\*a\*b\* values of the fired and repaired specimens were recorded.  $\Delta E$  values and translucency parameters ( $\Delta TP$ ) were calculated using initial and final recorded data. The acquired data was analyzed using two-way ANOVA.

**Results:** Mean  $\Delta E$  values of the groups were compared to clinical acceptability threshold ( $\Delta E=5.5$ ) and clinical detection threshold ( $\Delta E=3.7$ ). Group K1 (1 firing and Clearfil Repair) showed that lowest mean  $\Delta E$  value ( $\Delta E=3.57$ ) and this was within the clinical detection level. Other Clearfil Repair applied groups illustrated that clinically acceptable results related to clinical acceptability threshold. Mean  $\Delta E$  value of Ceramic Repair N applied groups were higher than clinically detection and acceptable levels. Highest mean  $\Delta E$  value ( $\Delta E=6.24$ ) was found at Group K7 among the tested groups. Translucency parameters ( $\Delta TP$ ) decreased while firing number increased.

**Conclusion:** Color of the repaired zirconia restorations might be affected by multiple firings and intraoral porcelain repair systems. Color differences of the groups that repaired using Clearfil Repair kit were clinically acceptable. Besides, if firing number of zirconia framework increases, color and translucency differences will be high after the repair.

## INTRODUCTION

Porcelain fused to metal restorations have been offered to patient as an option for fixed partial denture since 1960s<sup>[1]</sup>. The use of the metal as substructure increases strength and provides support, while the use of porcelain ensures

esthetics. However, opacity and dark color of the metal obstruct the reflection of the natural tooth color in the restoration [2].

Increased esthetic demands from the prosthetic restorations, requirement of the restorations that have similar optical properties to tooth structure are possible factors to trigger development of the all-ceramic restorations [3]. Alongside the esthetic advantages of all ceramic restorations need to be durable as well as porcelain fused to metal restorations. The all ceramic systems sufficiently resist to compressive stresses, whereas they are weak against to strain forces. Zirconia based ceramic restorations have been widely accepted in dental applications, due to superb biocompatibility and mechanical properties [4]. In recent years, more translucent zirconia monolithic systems have been introduced, but feldspathic porcelain veneered zirconia fixed partial dentures are still presented more esthetic results [5].

Clinicians usually prefer the zirconia based porcelain restorations that are fabricated using a CAD/CAM system for substructure, due to more accurate fit of the restorations [6]. Two different CAD/CAM techniques are frequently used in this manner. These are soft milling and hard milling techniques. Pre-sintered zirconia blocks are milled in the soft milling technique and the milled restorations shrink dimensionally 20% to 25% after the final sintering procedure. Completely sintered zirconia blocks are milled in exact dimensions of the restorations without any thermal or sintering process [7].

Zirconia substructure in zirconia ceramics obtains adequate strength for the restorations. Clinical follow-up studies proved that porcelain veneered zirconia restorations served successfully in oral environment without any complications up to 5 years [8,9]. However, incidence of fracture or chipping in the veneered porcelain is still high and the zirconia substructure can be exposed. This failures are frequently observed issues for zirconia ceramics [10]. Cause of damages may be induced by various factors in the zirconia based restorations. These are sintering procedure of zirconia and structural defects [11,12], airborne particle abrasion [13], planning of substructure [14,15], type of margin design [16], multiple firings [10,17-19], aging of zirconia [20] and luting procedure [21].

Remaking or repairing the failed restorations are probably primary treatment options when encountered to fractured porcelain. The failed restorations have to be removed from the mouth, but this is either time-consuming or open to complication. The restorations can be repaired using intraoral repair systems into the mouth. This technique may increase serving time of the restorations, save on the time and possible costs, and eliminate removal of the failed restorations for remaking or repairing [22].

The success of the intraoral repair systems affects from bonding between the composite resin and surface of the restoration [23]. Various surface treatment methods may be applied to the surface of failed restoration, in order to enhance bonding strength. Apart from the instructions manual, several surface treatment procedures were described in the literature such as, intraoral airborne particle abrasion, tribochemical silica coating, acid etching, short or long pulse of laser irradiation [18,23-25]. Esthetics and color harmony of the intraorally repaired restorations are important issue as well as strength of them. The clinicians easily restore shape and form of the failed restorations, but reflection of accurate shade on the restoration is a major drawback of this repairing method [26]. Thickness of veneered porcelain [27], number of firing [17,19,28], firing temperature and parameters [17,18], material of substructure [29] and applied surface conditioning method on the substructure [26], play key role on to final shade of the porcelain restoration.

Multiple firings during the preparation of the restoration can weaken the bonding between the porcelain and the zirconia, which may lead to fractures and chipping in the porcelain [10,18,30,31]. Beside to connection errors that prompt by repeated firings, porcelain color changes also stated that in the literature [17,19]. Color incompatibilities may occur between the repaired area and rest of the restoration.

The aim of this study was to evaluate color stability of repaired multiple fired zirconia substructures that were fabricated using CAD/CAM technology and repaired two different intraoral repair kit. The null hypothesis of the current study was that increasing number of firing has no effect on color differences of the repaired restoration.

## MATERIALS AND METHODS

Eighty disc shaped (5 mm diameter and 2 mm height) zirconia (ICE Zirkon Translucent, Zirkonzahn GmbH, Gais, Germany) specimens were fabricated using CAD/CAM system. Shade of the specimens was A1 according to Vita Classical Shade Guide (Vita Zahnfabrik H. Rauter GmbH & Co. KG) (**Figure 1**).

Color measurement of all specimens was performed over a black background using a digital spectrophotometer (Vita Easyshade Advance 4.0, Vita Zahnfabrik H. Rauter GmbH & Co. KG) under D65 light source. Measured values were recorded in CIE L\*a\*b\* system.



Figure 1. Prepared zirconia specimen for the study.

The specimens were devoted to two groups for different intraoral porcelain repair systems (Ceramic Repair N, Kuraray Noritake Dental Inc, Okayama, Japan, and Clearfil Repair, Ivoclar Vivadent AG, Schaan, Liechtenstein). This groups were sorted to four subgroups (n=10) regarding number of firing (1, 3, 5 and 7) (Table 1).

Table 1. Definition of the tested groups in the study.

Number of firings/repair system	Ceramic repair N	Clearfil repair
1 firing	Group C1	Group K1
3 firing	Group C3	Group K3
5 firing	Group C5	Group K5
7 firing	Group C7	Group K7

Specimens into the subgroups were fired using standard parameters of porcelain baking in the porcelain furnace. After the firing process, the specimens were repaired using related intraoral porcelain repair kits according to group. Dental composite resin of each repairing systems was applied to the specimens via teflon mold (2 mm x 2 mm). L\*a\*b\* values of fired and repaired specimens were recorded again over the black background (Figure 2). The ΔE values between zirconia and fired-repaired zirconia specimens were calculated with the formula.

$$\Delta E_{(L,a,b)} = [(L^*1-L^*2)^2 + (a^*1-a^*2)^2 + (b^*1-b^*2)^2]^{1/2}$$

Change in translucency was evaluated using ΔTP formula between color measurement (L\*a\*b\* values) over white and black backgrounds after the repairing procedures.

$$\Delta TP = [(L^*s-L^*b)^2 + (a^*s-a^*b)^2 + (b^*s-b^*b)^2]^{1/2}$$

The acquired data showed that homogeneity according to Shapiro-Wilk normality test of analysis of variance. (p<0.05) Two-way ANOVA statistical test was applied using a statistical software package program (PSPP 1.0.1, GNU, FSF Inc, Boston, MA, USA). Post Hoc test was used multiple comparison of the groups.

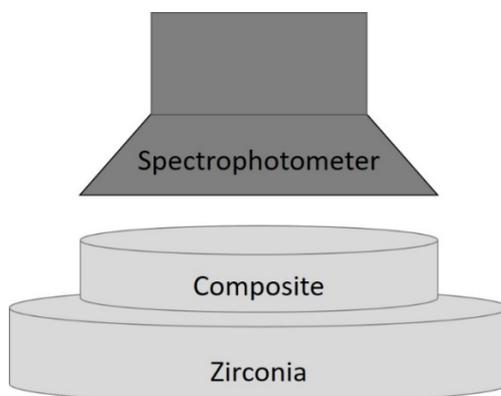


Figure 2. Diagram of the tested specimen and color measurement.

## RESULTS

If the  $\Delta E$  value is above 3.7, the color difference can be perceived by the eye. If the  $\Delta E$  value is above 5.5, the color difference is clinically unacceptable. The mean  $\Delta E$  values of the groups were compared with clinically detectable limit ( $\Delta E=3.7$ ) and clinically acceptable threshold ( $\Delta E=5.5$ ).

The lowest mean  $\Delta E$  value was found in Group K1 ( $\Delta E=3.57$ ), and this was under the clinically detectable limit. Also, other groups which applied Clearfil Repair kit illustrated lower than clinically detectable limit. The highest mean  $\Delta E$  value was observed in Group K7 ( $\Delta E=4.70$ ) (Table 2). The difference of mean  $\Delta E$  values between Group K1 and Group K7 was statistically significant.

The mean  $\Delta E$  values of groups that repaired Ceramic Repair N were higher than the clinically detectable and acceptable thresholds. The highest mean  $\Delta E$  value ( $\Delta E=6.24$ ) was seen in Group C7 among the tested groups. For the Ceramic Repair N applied groups, the lowest mean  $\Delta E$  value was found in Group C1 ( $\Delta E=6.07$ ) (Table 2). However, the differences between the mean  $\Delta E$  values of the Ceramic Repair N applied groups were not statistically significant.

According to the results of the statistical analysis, effects of the applied repair systems, number of firing, and the interactions between them were found to be significant.

$\Delta TP$  value were perceivable by the eye, if it was over 2.32 Mean  $\Delta TP$  values of Group C1 ( $\Delta TP=3.01$ ) and Group C3 ( $\Delta TP=2.07$ ) were observed higher than the perceptibility limit. Mean translucency parameter differences of the groups showed that lower values than the limit (Table 2). For the Ceramic Repair N applied groups, the differences between Group C1 and Group C5 and C7 were found statistically significant. Any statistically significant differences were seen among the Clearfil Repair applied groups.

The effects of the applied repair systems and number of firing were found to be significant with regard to statistical analysis of translucency parameter differences, but any significant differences were not observed at interactions between them.

Table 2. Mean  $\Delta E$  and  $\Delta TP$  values of the groups.

Groups	Mean Color Difference ( $\Delta E$ )	$\pm S. E.$	Mean Translucency Parameter Difference ( $\Delta TP$ )	$\pm S. E.$
Group C1	6.07	0.87	3.01‡	1.28
Group C3	6.12	0.60	2.07	1.58
Group C5	6.20	0.40	1.55	0.79
Group C7	6.24‡	0.77	1.59	0.87
Group K1	3.57*	0.97	1.64	0.89
Group K3	3.89	1.56	1.55	0.86
Group K5	4.42	1.26	0.90	0.38
Group K7	4.70	1.39	0.79*	0.44
<p>p&gt;0.05 *The lowest value of <math>\Delta E</math> and <math>\Delta TP</math> ‡The highest value of <math>\Delta E</math> and <math>\Delta TP</math></p>				

## DISCUSSION

In this study, the differences between the initial color of the milled zirconia specimens and the color after the repairing procedure, and the translucency were analyzed by applying two different intraoral porcelain repair systems and various numbers of firing. The null hypothesis of the current study was rejected. Color differences between the zirconia and the repaired zirconia with composite resin were found high related to number of firing. Similarly, mean translucency parameters were decreased parallel to number of firings of the zirconia specimens.

The most common failure reason in the zirconia ceramics is crack or chipping in the porcelain and zirconia substructure may come into the open oral cavity<sup>[10]</sup>.

Several studies stated that repetitive firings during the preparation weaken of the connection between the porcelain and the zirconia [10,18,30,31]. The bonding failure that is generated by multiple firings can also cause to color change in the restoration, beside to increased risks of fracture and chipping [17,19].

Possible factors that caused to failure should be considered, when the clinician faced to cracked or chipped restoration. Effect of multiple firings process should not be ignored to cause fracture of zirconia based porcelain restoration as well as the main factors, such as sintering procedure of zirconia, structural defects, type of margin design, etc. [10-21].

Vichi et al. [10] investigated effect of multiple firings on to flexural strength of zirconia ceramics, and reported that three firing processes significantly increased the strength. They suggested that to do 3 times baking instead of one baking, and also added that 5 times baking would be applied to achieve better esthetics and this did not significantly decrease the strength compared to 3 times baking. As stated by the authors, this is an undeniable fact that esthetic results are desired as well as the durability of the restoration. In the present study, esthetic features of the zirconia ceramics that were fired multiple times were evaluated after repaired with intraoral porcelain repair systems.

It was stated that in the literature, design of substructure, surface conditioning procedures and number of firing might affect final color of the porcelain restoration [17,19,26,28,29]. However, detailed information was not found about esthetic success of the intraorally repaired restoration in the literature. Esthetic outcome of the repaired restoration is extremely important on account of incident of porcelain fractures on the maxillary anterior region [32,33].

Kirmali et al. [24] concluded that application of various surface conditioning methods could enhance bonding strength between the restoration and the composite resin. Moreover, they advised that to follow instructions manual of the intraoral porcelain repair system. In the current study, intraoral porcelain repair kits were applied in the light of manufacturer's recommendations.

Correct definition of the color is key factor to fabricate restorations with color harmony. Success rate of the restoration can increase carefully selection of the shade [34]. Digital color measuring devices have several advantages compared to visual shade guide systems. The digital devices swiftly present objective data and enable to evaluate color in numerical values [34,35]. A study was conducted to analyze accuracy of spectrophotometer and success rate was reported as 83.3% [35]. Therefore, a spectrophotometer was used to objectively evaluate differences of color and translucency.

Gonuldas et al. [17] evaluated effects of repeated firings on the color stability and surface roughness of zirconia ceramics. They reported that increased number of firing caused to more rough surfaces and differentiation in the color. The authors concluded that the technicians should avoid multiple baking processes, when manufacturing the restorations.

Yilmaz et al. [19] investigated effects of different number of firing and various polishing techniques on the color features of all ceramic restorations. They found that the multiple firings caused to transformations in the crystalline structure. Thus, the authors reported that differentiations in the color of restoration might occur regardless of polishing techniques. In this study, color differences were observed after the repair parallel to number of firing, irrespective to applied intraoral porcelain repair kits and composite resins.

Color differences between the porcelain restorations and the composite resins for porcelain repairing were assessed by AlGhazali et al. [36] and they observed that  $\Delta E$  values were range from 3.5 to 26.9. Clinically acceptable threshold was applied as  $\Delta E=5.5$  in that study they suggested that to use combination of different colors of the composite resin instead of single shade of the composite in order to achieve perfect color match for repaired restorations. In the present study, the mean color change was observed within the clinically acceptable limit in the groups that applied Clearfil repair kit, but color changes for the Ceramic Repair N used groups were found above this level.

Limitations of this study were that the maximum number of repeated firings were 7, the other all ceramic materials were not involved in the study and the samples were prepared on the basis of single color.

Color change of the group that was fired one time and repaired using Clearfil Repair intraoral porcelain repair kit was under the clinically detectable limit ( $\Delta E=3.7$ ). Although color changes of the other Clearfil Repair system applied groups were above the clinically detectable limit ( $\Delta E=3.7$ ) and under the clinically acceptable limit ( $\Delta E=5.5$ ), statistically significant difference was solely found between the one firing and the seven firings applied groups. Translucency parameters ( $\Delta TP$ ) were showed decreasing trend parallel to number of firing regardless of applied intraoral porcelain repair kits.

## CONCLUSION

Color of the repaired zirconia ceramics can be affected by multiple firings and type of intraoral porcelain repair kit. The color changes of the groups repairing with the Clearfil Repair kit were clinically acceptable. But, the Ceramic Repair N

repair system applied groups were not within the clinically acceptable range. As if the firing numbers of zirconia substructures are increased, the color and translucency differences can be more after the repair. In addition, further *in vitro* studies and multicenter clinical trials are required investigating different intraoral porcelain repair systems and other all ceramic restorative materials.

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