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A Robust Algorithm for Retinal Blood Vessel Extraction

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ABSTRACT: Non-proliferative diabetic retinopathy (NDPR) detection is currently a highly interested research area. Ophthalmologists detect NDPR by observing disorders in the vessel system. Therefore segmentation of the vessel system will be an aid for ophthalmologist in order to detect an early retinopathy. In this proposed frame work a novel method based on Gabo Filter and adaptive thresholding has been used. The results have been tested using sensitivity and specificity and the values are 92.36% and 87.52% respectively.

KEYWORDS: Non-proliferative diabetic retinopathy, Vessel extraction, Gabor Filter, Local adaptive Thresholding, Binarization.

I. INTRODUCTION

Diabetic retinopathy is an eye disease that occurs due to a complication of diabetes which usually results in severe vision loss or permanent blindness. It occurs when high blood sugar levels damage the tiny blood vessels that nourish the retina. High blood sugar levels can cause the blood vessels to narrow down and as a result the constant supply of blood to the retina will reduce. There can also be leakages in blood vessels due to this issue. “Non-Proliferative Diabetic Retinopathy” (NDPR) is the early state of the disease. During this period, tiny bulges occur in the vessel walls. In order to monitor the early stages of retinopathy or “NDPR”, Ophthalmologists need to closely monitor the blood vessels in a retina. Hence, segmentation of blood vessels in a retinal image will ease the effort of the Ophthalmologists when finding the early stages of this disease. This paper proposes a novel method of extracting the vessel system from a retinal image.

II. RELATED WORK

The green channel of the original fundus image has been used to obtain the traces of blood vessels and morphological operations followed with enhancement, background exclusion and thresholding has been used to extract the vessels in the approach taken by S. Joshi and P.T.Karule[1]. In “Vessel Segmentation in Retinal Images using Graph-Theoretical Vessel Tracking” a vessel tracking technique based on seed points is used to extract the vessel system out of the retinal image [2]. Otsu thresholding and Medial Axis Skeletonization based method followed by pruning has been used in the research done by L.Sukkaewet *al* [3]. Next a complex Gabor filter is used to enhance the vessels and the result is further purified by using. entropic thresholding in the research done by P.C. Siddalingaswamy and K.G. Prabhu [4]. D.onkaew and B.uyyanonvara in “Automatic Extraction of Retinal Vessels Based on Gradient Orientation Analysis” [5] which has used a gradient orientation method to separate the vessel system.

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III. PROPOSED ALGORITHM

The proposed methodology can be divided into six steps. The following flow chart shows the steps in the methodology of the proposed algorithm.

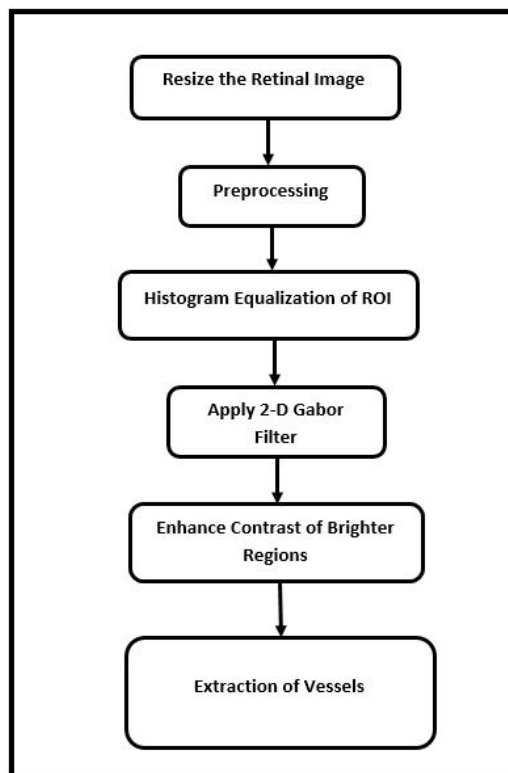


Fig1 : Steps in the Proposed Methodology

A. Resizing the Retinal Image

Various different sizes of color retinal images are brought to one common 600x600 size in order to bring them in a common dimension.

B. Pre-processing

In the retinal images, the blood vessels show a higher contrast in the green channel than the red channel or the blue channel. Only the extracted green channel of the retinal image will be further processed [6]. A 2-D median filter with a 3-by-3 neighborhood is applied, in order to eliminate the noise of the green channel image. In the processed image each output pixel contains a median value in the 3-by-3 neighborhood around the particular pixel in the input image [7].

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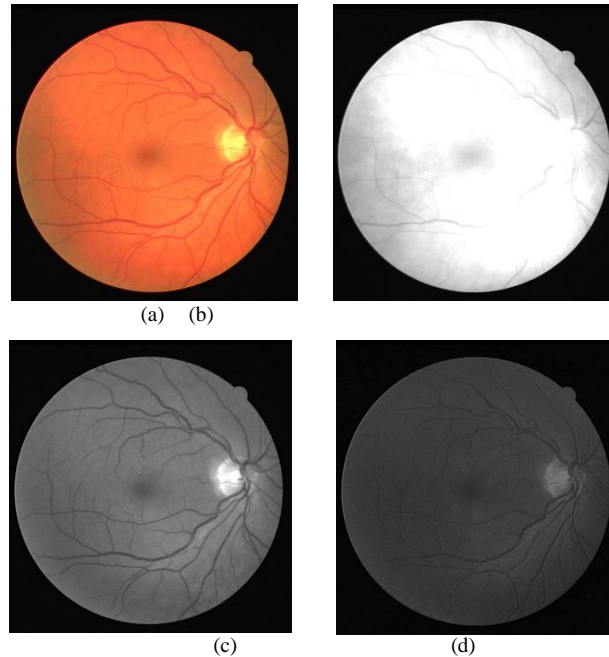


Fig2 : Extraction of RGB Image: (a) input RGB Image (b) Red Channel Component (c) Green Channel Component (d) Blue Channel Component.

C. Histogram equalization retinal ROI

The ROI (Region of Interest) in the fundus image is the retinal area (the area without the background). Histogram equalization is an efficient image enhancement procedure to change the mean brightness of an image using its histogram to change to the middle level of the permitted range [8]. In this proposed research, the histogram equalization is performed to change the pixel intensities of the green channel to enhance the contrast of the retinal blood vessels in the image.

The equalized histogram of the source image $h(x)$ is represented as a x_r -by- x_c matrix and pixel intensities ranging from grey level 0 to level $L-1$. Furthermore, $cdf(x)$ is the cumulative density function of the green channel image and $cdf_{min}cdf_{max}$ are the lowest and the highest integer values of the $cdf(x)$.

$$h(x) = round\left(\frac{cdf(x) - cdf(\min)}{(x_r \times x_c) - cdf(\min)} \times (L - 1)\right) \quad \text{eq. (1)}$$

In the proposed algorithm, histogram equalization is only applied to the ROI of the retinal image in order to get equalized distribution. This is done to reduce the variation of the intensity values of each pixel.

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Fig3 : The Enhanced Green Channel using Histogram Equalization

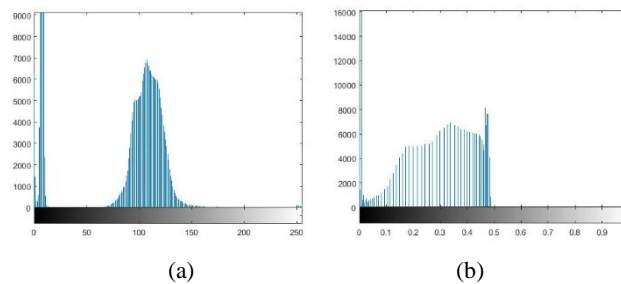


Fig4: Green Channel Histogram (a) Before Equalization (b) After Equalization

D. Apply 2-D Gabor Filter

The 2-D Gabor filter is a linear filter, that has been widely used for low level oriented edge detection and extraction of texture features for discrimination purposes in image processing and computer vision fields. Frequency representation and orientation representation of the Gabor filter are identical to the human vision system. In the spatial domain, a 2-D Gabor filter is a Gaussian kernel function modulated by a sinusoidal plane wave [9]. Enhancement of the pixels of the blood vessels oriented along the various dimensions can be done due to the factor of directional selectivity of the Gabor filter. The response of the Gabor filter is a complex number with real and imaginary parts that are orthogonal and act as low level oriented edge discriminators [10] [11].

The equalized image is complimented (inverted) and Gabor filter is applied to highlight the blood vessel vascular system, by ignoring the background noise. The filter has a real component as well as imaginary component expressing orthogonal directions. The two components of real part and imaginary part can be formed into a complex number represented by,

$$g(x, y; \lambda, \theta, \psi, \sigma, \gamma) = \exp\left(\frac{-x'^2 + \gamma^2 y'^2}{2\sigma^2}\right) \exp\left(i\left(2\pi \frac{x'}{\lambda} + \psi\right)\right) \quad \text{eq. (2)}$$

Individually the real component represented by,

$$g(x, y; \lambda, \theta, \psi, \sigma, \gamma) = \exp\left(\frac{-x'^2 + \gamma^2 y'^2}{2\sigma^2}\right) \cos\left(2\pi \frac{x'}{\lambda} + \psi\right) \quad \text{eq. (3)}$$

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Imaginary component is given as,

$$g(x, y; \lambda, \theta, \psi, \sigma, \gamma) = \exp\left(\frac{-x'^2 + \gamma^2 y'^2}{2\sigma^2}\right) \sin\left(2\pi \frac{x'}{\lambda} + \psi\right) \quad \text{eq. (4)}$$

Where,

$$x' = x \cdot \cos(\theta) + y \cdot \sin(\theta) \quad \text{eq. (5)}$$

$$y' = -x \cdot \sin(\theta) + y \cdot \cos(\theta) \quad \text{eq. (7)}$$

The Gabor filter depends on the a few parameters. The parameter θ exemplify the orientation of the filter. λ represents wavelength of the sinusoidal function and ψ is the phase offset. σ is the variance of the Gaussian envelope. When σ changes, Gabor filter with above parameters does not scale uniformly. Thus, it is better to use parameter $\gamma = \frac{\lambda}{\sigma}$ instead of λ . Where γ is the spatial aspect ratio which specifies the ellipticity of the support of the Gabor function. By selectively changing the above parameters (γ, θ, σ) a clear response of vessels could be obtained.

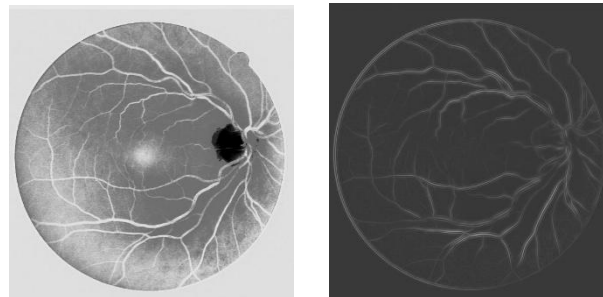


Fig5: Apply 2-D Gabor Filter (a) Inverted input image (b) Gabor Response image

E. Enhance Contrast of Brighter Regions

After applying the Gabor filter, further enhancement of the pixel contrast is done by using 'raise to power' operator, which is an anamorphosis operator that can be applied to the grayscale images to enhance contrast of the brighter regions.

The 'raise to power' operator is an individual point process where each pixel intensity value is replaced according to the basis value of the input image. The input image is raised to a certain value according to the mapping function.

The operator is defined as follows,

$$Q(x, y) = c \cdot P(x, y)^r \quad \text{eq. (7)}$$

Where, $P(x,y)$ and $Q(x,y)$ are the pixel intensity values of the input image and the processed image respectively. ' c ' is the scaling factor and ' r ' is a fixed value. The operator is also known as 'gamma correction. It is a nonlinear method for adjusting the overall luminance of an image [12].

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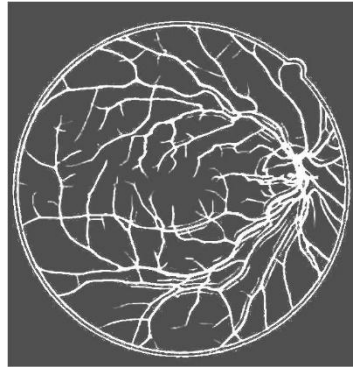


Fig6: Enhance Contrast of Brighter Regions

F. Extraction of Vessels

The enhanced image after applying the 'power to ratio' operator, an effective thresholding technique is required to extract the blood vessels structure from the retinal image. At this stage global thresholding method cannot be applied due to the various gray levels at various regions in the image. The processed image is a matrix with M rows and N columns. Then window concept is used to convert the image into binary tone.

In the proposed methodology, the Sauvola's local binarization method is used to extract the vessel vascular system. The local binarization method calculates a threshold value for each and every pixel in the window rather than using a global threshold value. In Sauvola's binarization method, the pixel threshold value $T(x,y)$ is computed using the mean $\mu(x,y)$ and the standard deviation $\sigma(x,y)$ of the pixels in a window size of $M \times N$ [13][14].

Sauvola's binarization method,

$$T(x, y) = \mu(x, y) \left[1 + k \left(\frac{\sigma(x, y)}{R} - 1 \right) \right] \quad \text{eq. (8)}$$

Where R and K is the maximum standard deviation value and a bias value in the range of 0.2 to 0.5 respectively. After the binarization process, it is necessary to remove the noise. In order to get a clear image, unconnected pixels smaller than in size of 30 are removed.

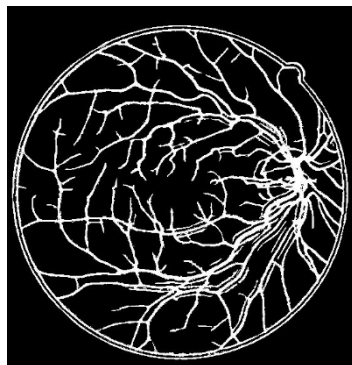


Fig 7 : Final Segmented Image

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IV. SIMULATION RESULTS

The proposed algorithm was tested with an open source data set named “DRIVE”. This data set contains 20 images in the size of 565x584 pixels. The sensitivity and specificity have been obtained based on the ground truth data available in the Drive data set. The obtained results are compared with [5]. A “Sensitivity” vs “1-Specificity” plot or in other words “ROC” curve (receiver operating curve) is taken in order to compare with [5]. The four metric values for Sensitivity and Specificity calculations are given as follows,

- True Positive – Sum of pixels identified as vessels similar to the ground truth image.
- False Negative – Sum of pixels which are vessels in the ground truth image but identified as background.
- True Negative – Sum of pixels which is identified as background just as in the ground truth image.
- False Positive - Sum of pixels which are background in the ground truth image but identified as vessels.

The Sensitivity and Specificity calculations are done according to the following formulas,

$$\text{Sensitivity} = \frac{\text{True Positive}}{\text{True Positive} + \text{False Negative}} \quad \text{eq. (9)}$$

$$\text{Specificity} = \frac{\text{True Negative}}{\text{True Negative} + \text{False Positive}} \quad \text{eq. (10)}$$

The Sensitivity of the proposed framework is 92.36% and the Specificity is 87.52%. Therefore the results are clearly better than the Sensitivity and Specificity values given in [5]. The “ROC” curve is given below (figure 8). The ROC curve of the proposed algorithm and the method given in [5] (GOA method) are compared in the following figure.

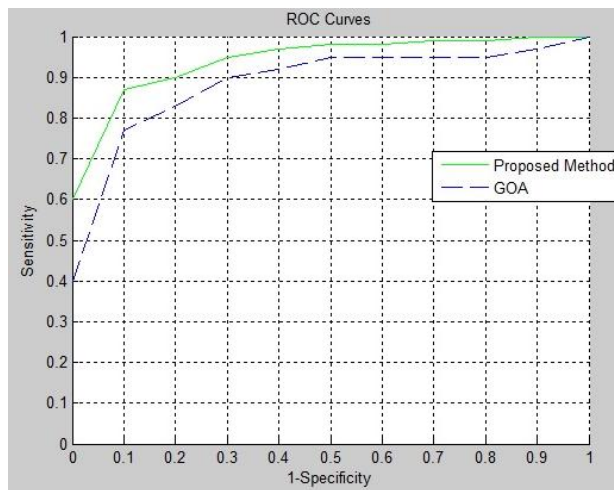


Fig 8 : Comparison between the proposed method and GOA

The area under the “ROC” curve signifies the discriminatory ability of the algorithm. Therefore when the area of the curve increases the accuracy of the vessel segmentation algorithm increases. Therefore according to the above graph the proposed algorithm is better than the “GOA” method given in [5]. The first column of Fig 9 shows the retinal fundus images. The second column brings out the manual segmentation images and the third row presents the results of the proposed algorithm.

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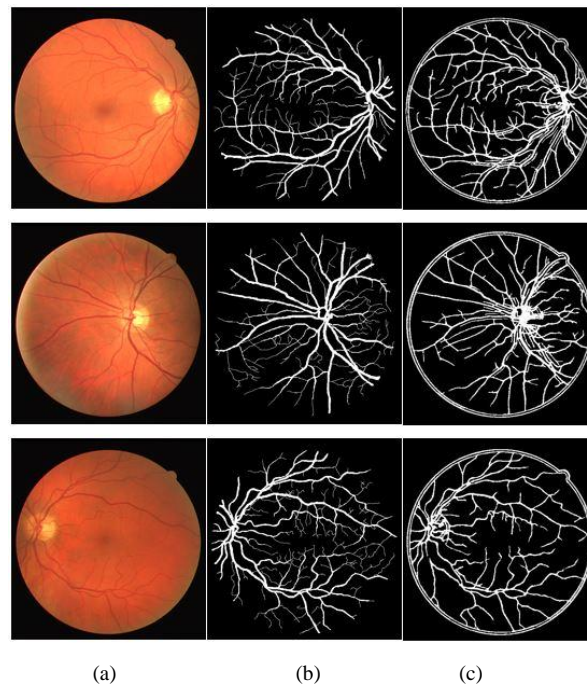


Fig 9 : Retinal Vessel Segmentation (a) Image from DRIVE Database (b) Manual Segmentation (c) Proposed Method Results

V. CONCLUSION

A method based on histogram equalization and Gabor filter to extract the retinal vessels in fundus images was represented by the proposed work. The performance of the proposed methodology is evaluated on the DRIVE database. The results were tested using sensitivity and specificity. They were more accurate than the method given in [5].

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BIOGRAPHY

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