Frequency Dependent Attenuation of EM Radiation on Biological Tissues

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ABSTRACT: The human body is a non-homogeneous medium and it is characterized by different fundamental parameters. All of them vary from location to location. Human body acts as a transmission medium for electrical signals. This offers novel data communication in biomedical monitoring systems. The human body is characterized as a transmission medium for electrical current by means of numerical simulations and measurements. Several attempts have been made to model the human body as electrical channel. Here the variations of penetration characteristics of the Electromagnetic radiation of the biological tissues had been observed.

KEYWORDS: Non-homogeneous medium, transmission medium, Electromagnetic radiation, penetration characteristics, biological tissues, electrical current

I. INTRODUCTION

It is common practice to study the behavior of electromagnetic waves in homogenous medium. In order to apply electromagnetic energy for the treatment of different tumors, the characteristics of the biological tissues are required to be established. It is well known that the homogenous media is characterized by constant values of permittivity, permeability and conductivity throughout the medium. On the other hand, non-homogeneous medium is a medium for which the above fundamental parameters are not constant and are different from point to point in the media. The human body is a non-homogeneous medium and it is characterized by different fundamental parameters. Using the novel data communication in biomedical monitoring systems [6]. The hyperthermia treatments are categorized as a whole body, regional or local. The rational for the whole body hyperthermia is that the cancer is a systemic disease and the cancer cells have metastasized throughout the body in most of the cases. It has been possible to find out relative electromagnetic energy absorption characteristics of the data on fundamental constants of the tissues. In order to apply electromagnetic energy as a function of frequency, The equivalent and simplified circuit(Fig. (a)) for a cell or a tissue [7].

![Fig. (a)](image)

Rₑ = extracellular fluid resistance
Rᵢ = intracellular fluid resistance
Cₘ = cell membrane capacitance

In the presence of an electromagnetic field, the biological tissue is considered as a medium with losses [8], [9], [10], [11], [12]. At frequency ω of complex electric field E⁺→and complex magnetic excitation H⁻→ the Ampere law [13] is given by:
The complex permittivity $\varepsilon'$ characterizes the biological tissue with conduction losses, and can be written in the following form [9], [11], [12]:

$$\varepsilon' = \varepsilon (\varepsilon' - j\varepsilon'')$$

Where $\varepsilon_0 = 8.88 \times 10^{-12}$ F/m is the absolute permittivity.

$\varepsilon' = \frac{\varepsilon}{\varepsilon_0}$ and $\varepsilon'' = \frac{\sigma}{\omega\varepsilon_0}$ are the relative permittivities with the conductivity $\sigma$ and the dielectric permittivity $\varepsilon$ of the biological tissue. $\varepsilon'$ and $\varepsilon''$ are often indirectly measured by using RF impedance bridges and are provided into tables as a function of the frequency [9], [11]. A new approach is adopted here to evaluate the power attenuation caused by the presence of a biological tissue between the transmitter and receiver coupled coils. The magnetic field propagation in the biological tissue which is defined by its parameters of permittivity $\varepsilon$, conductivity $\sigma$ and permeability of vacuum $\mu_0$, is according to the magnetic wave equation, [13], using the Laplacian operator $\nabla^2$:

$$\frac{1}{\mu_0} \nabla^2 \vec{B} = \frac{\sigma}{\omega \mu_0} \frac{\partial \vec{B}}{\partial t} - j\omega \varepsilon \frac{\partial^2 \vec{B}}{\partial t^2}$$  \hspace{1cm} (3)

For a sinusoidal variation of magnetic field $\vec{B} = \vec{B} e^{j\omega t}$ Equation (3) becomes:

$$\nabla^2 \vec{B} = j\omega \mu_0 (\sigma + j\omega \varepsilon) \vec{B} = \gamma^2 \vec{B}$$  \hspace{1cm} (4)

where $\gamma^2 (m^{-1}) = \alpha + j\beta$ is the propagation constant and $\alpha$, $\beta$ are attenuation and phase constants, respectively.

$$\alpha = \omega \sqrt{\frac{\mu_0 \varepsilon}{2} \left(1 + tg^2 \delta - 1\right)}$$  \hspace{1cm} (5)

$$\beta = \omega \sqrt{\frac{\mu_0 \varepsilon}{2} \left(1 + tg^2 \delta + 1\right)}$$  \hspace{1cm} (6)

The losses of the medium are represented by the tangent of loss [7].

$$tg \delta = \frac{\varepsilon''}{\varepsilon'} = \frac{\sigma}{\omega \varepsilon}$$  \hspace{1cm} (7)

**Tissue Characteristics of Human Body**

The attenuation constant in the biological tissue is a function of frequency, conductivity, permittivity and permeability of the bio-tissue. When an EM wave is allowed to incident on the tissue in such a way that electric field is parallel to the interference between the tissues, two adjacent tissues absorb power. Under these conditions, the electric fields are tangent to the interference between the pair of tissues and they are equal. When the electric fields are perpendicular to the interface, the conduction and displacement current becomes continuous across the interference. The following cases are considered for finding at the relative absorption of EM energy. The electric field vector parallel to the interference between the tissues. The electric field vector perpendicular to the interference between tissues.

**II. RESULTS**

The attenuation constant of a non-homogenous medium [human body] is evaluated by the expression (8)

$$\alpha = \omega \sqrt{\frac{\mu_0 \varepsilon}{2} \left[1 + \frac{\sigma^2}{\omega^2 \varepsilon^2} - 1\right]}$$  \hspace{1cm} (8)

Using the expression (8) the attenuation constant for different mediums like dry skin, wet skin, fat, muscle and cortical bone and bone marrow and the corresponding figures [1-6(c)] with respect to frequency varying from 10 KHz to 1GHz.
In Fig. 1(a), it is observed that the conductivity is very low at lower frequencies and while going towards the high frequencies the conductivity increases with increase in frequency.
In Fig. 1(b), the permittivity of dry skin tissues is observed to be high at low frequencies and gradually decreases with increase in the frequency.
In Fig. 1(c), the minimum attenuation of electromagnetic radiation by the dry skin tissues is observed at the frequencies around 10 KHz and maximum attenuation at around 10 MHz.

In Fig. 2(a), it is observed that the conductivity is linearly increasing with the increase of frequency of radiation.
In Fig. 2(b), the permittivity of wet skin tissues is observed to be high at low frequencies and gradually decreases with increase in the frequency.
In Fig. 2(c), the maximum attenuation of electromagnetic radiation by the wet skin tissues is observed at the frequencies around 1MHz.
In Fig. 3(a), it is observed that the conductivity takes place even at the low frequencies and also increases with frequency.
In Fig. 3(b), the permittivity of fat tissues is observed to be high at low frequencies and gradually decreases with increase in the frequency.
In Fig. 3(c), the maximum attenuation of electromagnetic radiation by the fat tissues is observed at the frequencies around 10 KHz.

In Fig. 4(a), it is observed that the conductivity takes place even at the low frequencies and also increases with frequency.
In Fig. 4(b), the permittivity of muscle tissues is observed to be high at low frequencies and gradually decreases with increase in the frequency.
In Fig. 4(c), the maximum attenuation of electromagnetic radiation by the muscle tissues is observed at the frequencies around 10 KHz.
III. CONCLUSION

Thus variations of the penetration characteristics such as conductivity and relative permittivity are plotted at various frequencies. From these we can obtain the attenuation of Electromagnetic radiation on different biological tissues such as skin, fat, muscle, corticle bone and bone marrow at the corresponding frequency range of 10KHz to 1GHz.
REFERENCES


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